



stress intensity factor (for the different crack propagation modes)  $K \equiv K_{LEFM}$  that must reach a critical value (the fracture toughness of the material,  $K_C$ ) for crack propagation, but instead the square root of the mean value of the square of the stress intensity factor along a fracture quantum, which is by definition the quantized stress intensity factor  $K_{QFM}$ . This theory is thus based on the removal of the hypothesis of continuous crack growth, i.e. on the existence of a quantum of energy dissipation/crack advancement, as postulated in the stress-analogue approach by Novozhilov [3]. In dynamic fracture, and considering the existence of a quantum of action, the mean value must be considered also along a quantum of time  $\Delta t$  -thus defining the dynamic quantized stress intensity factor  $K_{DQFM}$  [4]- as introduced again by the Russian's School in the stress-analogue incubation time fracture mechanics approach [5].

The exponent of 2 can in principle be generalized to a positive real number  $\alpha$ , thus proposing a Griffith/Generalized (Dynamic) Quantized Fracture Mechanics (GQFM), predicting crack propagation according to:

$$K_{GQFM}^{(\alpha, \Delta A, \Delta t)} \equiv \sqrt[\alpha]{\frac{1}{\Delta A \Delta t} \int_{t-\Delta t}^t \int_A^{A+\Delta A} K(A, t)^\alpha dA dt} = K_C \quad (1)$$

Note that  $K_{GQFM}^{(\alpha, \Delta A=0, \Delta t=0)} = K_{LEFM}$ ,  $K_{GQFM}^{(\alpha=2, \Delta A, \Delta t=0)} = K_{QFM}$ ,  $K_{GQFM}^{(\alpha=2, \Delta A, \Delta t)} = K_{DQFM}$  and  $K_{GQFM}^{(\alpha=1, \Delta A=0, \Delta t)} = K_{ITFM}$ , where  $K_{ITFM}$  is the equivalent stress-intensity factor according to the incubation time fracture mechanics [5]. Accordingly, all these limiting-case theories, which have been proved to capture experimental observations that LEFM cannot describe, are recovered and thus the correspondence principle is satisfied, as expected in the limit of vanishing fracture energy and action quanta.

The generalized stress intensity factor in (1) could also extend stress-intensity factor based laws such as those of fatigue, as proven for  $\alpha = 2$  to capture both long and short crack behaviours even in fatigue (thus from the Wöhler to the Paris regimes) [6]. With the criterion (1), apparent R-curve behaviours and strain-rate effects emerge naturally as a consequence of the existence of fracture and time quanta, rendering fracture toughness no longer, or less crack-length and strain-rate dependent, and thus a more realistic material property, as it must be by definition. This could also help in the formulation of more realistic Ashby's plots.

### MULTISCALE 3D ASHBY'S PLOTS

Ashby's plots are fundamental for material selection [7]. As is well known, simply assuming in Griffith's theory a crack length  $a \propto l^k$ , where  $l$  is the structural size, would result in a scaling law for the strength of the type  $\sigma \propto l^{-k/2}$ , as similarly predicted by Weibull's statistics [8] or by other interpretations, e.g. fractal geometry [9]. I do not wish to comment here about the details of size-effect laws, but rather to emphasize that with the advent of nanotechnology, it is not infrequent to see papers reporting the fabrication of a new material using an Ashby's plot, even if it has been tested at a smaller size-scale. The need to adopt different Ashby's plots at the micro- and nano-scales has already been highlighted [10]. Here, I propose to use 3D Ashby's plots for an improved multiscale representation, material/structural selection and comparison.

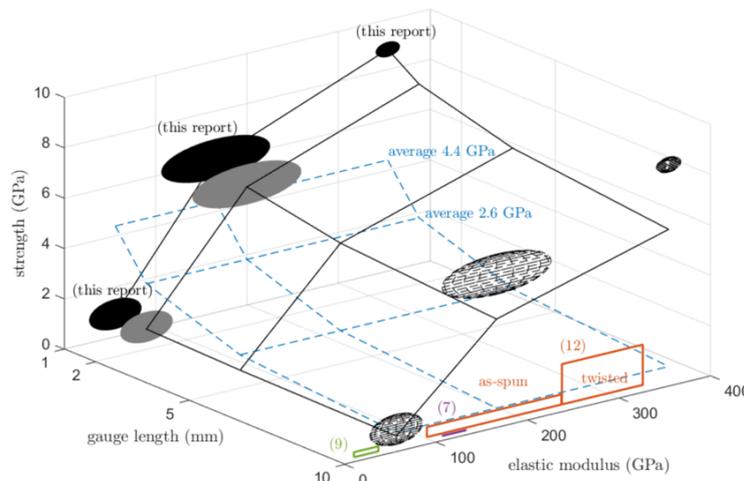


Figure 2. The black ellipses represent the strength vs elastic modulus data collected by the authors in [11] corresponding to samples with 1-mm gauge length (their fig. 4B). The overall average of this data is 4.4 GPa, while I have computed a total average of 2.6 GPa for the data at 2-mm gauge length (their fig. 3A). The corresponding scaling law, considering in a first approximation the independence of the elastic modulus, is of the type  $\sigma \propto l^{-k/2}$  with a large value of  $k/2 \cong 0.75$  (blue dashed lines). This scaling law predicts strength values comparable to those taken from the literature (green, purple or red areas, 1-cm gauge length). When considering the low- and high-strength regions (peaks in their fig. 3A), the average for the ellipse centred at a strength of 6.2 GPa for 1-mm gauge length falls to 5.6 GPa for a 2-mm gauge length, thus giving a scaling law with  $k/2 \cong 0.15$  (black solid lines). The dashed ellipses are the projections at 10-mm gauge length of those at 1-mm gauge length, as reported in [11], whereas mean or maximal predictions at 10-mm are those reported with the blue dashed or black continuous lines, respectively. This case study must be considered just a preliminary example, such as the deduced size-effects.

As an example, I treat the case reported in Figure 2, where nanotube bundles are considered according to the paper in [11]. Asbhy's plot presented by the authors was inevitably classical, i.e. 2D, without considering the role of the bundle/gauge length, even if these authors perfectly recognized the role of size-effects and thus tested samples at different gauge lengths. A 3D Asbhy's plot, with a new axis corresponding to the size-scale (here gauge length) could thus be a better choice for comparison with other experiments, as described in Fig. 2. The experiments from the literature reported for comparison in [11] were performed at a gauge length of 1 cm, which I have considered in the 3D plot. I have also reported their experiments [11], not in the same plane but in their correct positions (1-mm or 2-mm gauge length planes). According to the same authors' experiments at different gauge lengths and assuming the simple mentioned scaling law of  $\sigma \propto l^{-k/2}$ , I could predict mean or maximal strength values expected at larger gauge lengths, including 10 mm, as reported respectively with the blue dashed or black solid lines.

The need for multiscale 3D Asbhy's plots is thus evident if we wish to move towards a standardization in material property comparisons. Regarding fracture toughness, the use of criterion (1) could further help the standardization, as previously mentioned. In general, the understanding of the toughness mechanisms is fundamental in Nature and Engineering. We believe that we have discovered a new fundamental one in bones.

### A RECENTLY DISCOVERED TOUGHENING MECHANISM IN BONES

Bone tissue is a hybrid material made of an inorganic calcium phosphate phase nucleated into a collagenous matrix and organized hierarchically, from nanofibrillary components, to osteons (hundreds of micrometers in size), up to the cortical/trabecular macrostructure. It behaves as a complex composite able to adapt its internal organization to optimize the mechanical response under externally applied loads, contemporarily minimizing weight and resisting severe impacts and fatigue stress cycles by exhibiting surprising and not yet completely understood crack arresting mechanisms to avoid catastrophic fracture. In particular, it seems to be suitably designed to resist fracture at multiple size scales, thus achieving remarkable strength and toughness. However, the exceptional mechanical properties of bone can deteriorate with ageing and/or diseases: therefore, it is necessary to fully understand the mechanisms that confer these properties, also to develop therapies able to preserve or even rescue tissue functionality. Osteons, the fundamental bone units (Fig. 3a), are nearly hollow cylinders made of several concentric layers (lamellae) comprising helically arranged fibres wrapped nearly alternately clockwise and counterclockwise. With the Basic Multicellular Unit (BMU) osteocytes sense mechanical signals and activate and coordinate osteoblasts and osteoclasts for bone remodelling, i.e. resorption of preexisting bone by osteoclasts followed by *de novo* bone formation by osteoblasts (this process being impaired during ageing and diseases). It is ascertained that micro-damaging occurring across the scales plays a crucial role in bone mechanobiology, the micro-cracks opening at the osteon-matrix interfaces and within osteons working to trigger the BMU activities and the level of damage being an indicator of the need to locally increase mineral content through bone remodelling processes. However, how the crack propagation is triggered and arrested nearly simultaneously, both in compression and in tension (and thus also in bending) in such a stiff material, is still a partially unsolved enigma.

The most recognised hypothesis to explain the crack stopping/slowing phenomenon is based on the material inhomogeneity and anisotropy and the layered architecture of osteons: after nucleating, cracks would be halted when radially travelling across the osteon lamellae since they encounter the nearly alternating and in any case different arrangement of the wrapped fibres that make them decelerate at the lamellar interfaces and deviate along the circumferential direction. This leads to the dissipation of energy by increasing the length of the crack path, as well as by breaking micro-bridge elements and encountering a number of micro-voids and discontinuities generating micro-cracking. This mechanism surely plays an important role in arresting cracks in bone, but both theoretical calculations to estimate stress intensity factors at the crack tips and numerical analyses simulating crack propagation within osteons under static/cyclic loads as well as experimental findings [12], highlight that this is not sufficient to hinder fracture, suggesting that some yet undiscovered mechanisms should cooperate with (or exploit) bone hierarchy to halt crack progression [13]. Theoretical results also suggest that tensile hoop stresses in the lamellae, responsible for micro-crack opening in the radial direction, would occur only in case of compressive loads, while experimental observations show diffuse radial micro-cracks generated by tensile loads too [14].

Motivated by these incomplete and somehow contradictory results, we (the authors of ref. [15]) deeply explored an additional crack opening and stopping thus smart toughening mechanism with respect to those widely accepted in the literature, for which we have now clear theoretical evidences as well as experimental confirmation on 3D printed artificial hierarchical bones. For the occasion of this XXV ICTAM conference, we have rendered the paper public in the *Arxiv* [15]. Our results, obtained from an accurate mechanical model (Fig. 3a) of elastic anisotropy (Fig. 3b), show a counterintuitive radially distribution alternating in sign of both hoop and shear stresses in the lamellae and sub-lamellae (Fig. 3c,d), which could simultaneously act to open and halt cracks (Fig. 3e) thanks to hierarchy and symmetry breaking (Fig. 3f). This could also better stimulate the osteocyte activity by amplifying the mechanical signal, thus finally producing a "perfect" system capable to work both under compression or tension and thus bending.

Accordingly, this indeed unveils a powerful crack opening and simultaneously arresting mechanism, mediated by both the helical microstructure of the collagen fibrils in lamellae and sub-lamellae and the currently neglected small discrepancy in the nearly symmetric staggered angles of their wrapping in adjacent lamellae/sub-lamellae. The latter symmetry breaking generates this mechanism of Alternating Stresses in Lamellae (ASL, Fig. 3f), also occurring in sub-lamellae (ASL2) and hierarchy is shown to further enhance its power (Fig. 3c,d). Thus if ASL plays a fundamental role in bone toughening, its disappearance could be strictly related with bone ageing and common bone degenerative diseases, such as osteoporosis. Therefore, investigating the mechanosignaling pathways linking ASL to cellular response(s) and

tissue remodelling could have important and wide-ranging implications for both the comprehension of bone disorders and the conception of new therapies, essentially based on the idea of restoring ASL when lost. Additionally, with this ASL<sub>n</sub>-based toughening mechanism, a new design of bio-inspired *n*-level hierarchical composites is envisioned, e.g. in the next generation of self-healing materials where both crack opening and arrest could be required.

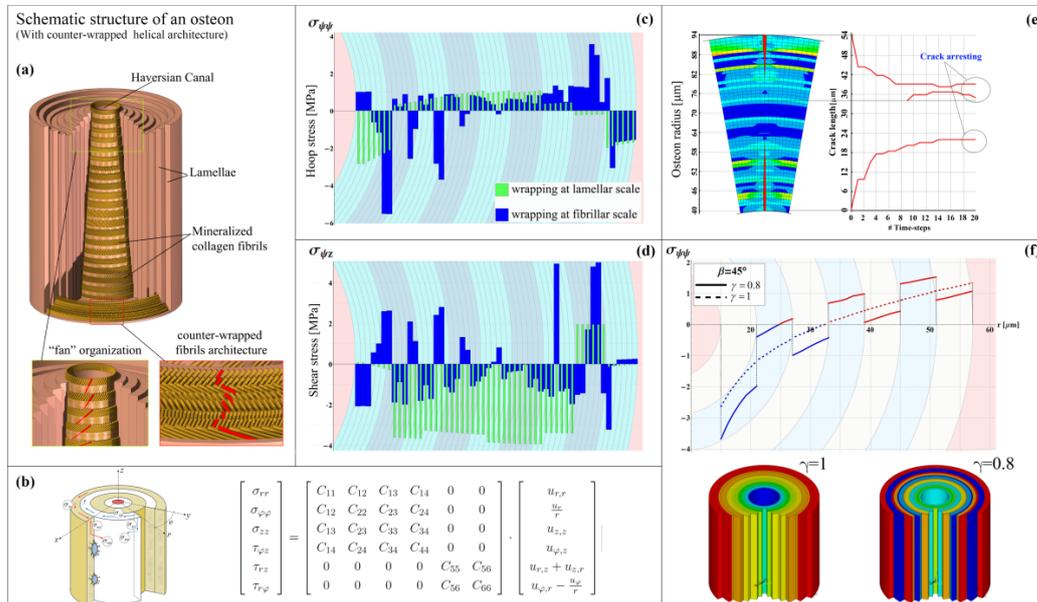


Figure 3. a) Osteon schematic structure. b) Anisotropic (monoclinic) elastic global equations resulting from the local helicoidal transversal isotropy (5 elastic constants). c-d) Alternating in sign hoop and shear stresses without or with the presence of sub-lamellae, with stress jump amplification in the latter hierarchical case. e) Numerically (finite element) simulated crack progression and halting across osteon lamellae. f) Alternating in sign hoop and shear stresses in adjacent lamellae with fibril wrapping angles of  $\beta$  and  $-\gamma$  respectively and related stress jump amplification for symmetry breaking ( $\gamma \neq 1$ ). For details see [15].

## CONCLUSIONS

To celebrate the centenary of Griffith's theory (1921), in this paper -related to the opening plenary lecture at XXV ICTAM- I have presented 3 new concepts in the field of fracture: (i) a new extension of Griffith's theory, following the previous proposals by the author on Dynamic/Quantized Fracture Mechanics; (ii) the proposal of multiscale 3D Ashby's plots, to include in these plots the fundamental role of the size-scale on the strength and in general on the mechanical properties of materials, for an improved material/structural selection and comparison; (iii) a new fundamental bone toughening mechanism, deriving from evidence of stress alternating in sign in osteon lamellae, emerging from the rupture of the symmetry of fibrils and empowered by hierarchy of sub-lamellae, suggesting also inspired solutions in Leonardo da Vinci's spirit [16].

As our lamellae, alone we are fragile but altogether we are resilient: this is why the pandemic is not stopping us, thanks to the new frontiers of Science and Technology and especially solidarity among peoples.

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